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Programa de Pós-Graduação em Biotecnologia



Tese

Partículas magnéticas: síntese e aplicações em ensaios de imunoseparação

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Pelotas, 2011.

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Partículas magnéticas: síntese e aplicações em ensaios de imunoseparação

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RESUMO

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O desenvolvimento de insumos para o diagnóstico e prevenção de doenças infecciosas é estratégico para o avanço científico e tecnológico do país. Resultados promissores vêm sendo obtidos com o uso de nanocompósitos magnéticos (NCM) aplicados à área da saúde para as mais diversas finalidades, como na separação, purificação e detecção de células ou biomoléculas. Nesse trabalho, um método de imunoseparação magnética (IMS) utilizando NCM a base de carbono e cobalto (NCMc) sintetizados, e outro de poliestireno e ferro (NCMp) disponível comercialmente, foi utilizado para capturar e detectar leptospiras patogênicas. Os NCMc foram sintetizados através do método dos precursores poliméricos e caracterizados por microscopia eletrônica de varredura/transmissão (MEV/MET), difratometria de raio-X (DRX), espectrometria no infravermelho (FTIR) e imunofluorescência (IF). A superfície dos NCMc foi funcionalizada com grupos carboxílicos mediante incorporação de ácido acrílico. Os NCMc adsorvidos com anticorpos monoclonais (MAbs) contra leptospiras patogênicas, quando utilizados em ensaios de IMS seguidos por PCR e cultivo celular, foram capazes de detectar e isolar o organismo. Os NCMp foram utilizados para a detecção de *Leptospira* spp. em fluidos biológicos de cães artificialmente contaminados com leptospiras e em amostras clínicas de cães positivos para a leptospirose. A introdução da IMS como passo anterior a PCR utilizando os NCMp foi capaz de detectar uma concentração 10 vezes menor de leptospiras quando comparada a PCR realizada diretamente a partir de amostras de urina e sangue artificialmente contaminados. Além disso, a IMS realizada com os NCMp aumentou a sensibilidade da PCR em amostras clínicas de cães positivos para leptospirose. Os dados obtidos em ambos os estudos sugerem que os NCMc e NCMp constituem importantes ferramentas para o desenvolvimento de novos testes de diagnóstico.

Palavras-chave: Diagnóstico. Cobalto. *Leptospira*.

ABSTRACT

Monte, Leonardo Garcia **Magnetic particles: synthesis and applications of immunoseparation assays** 2011. 61f. Thesis (Doctoral Degree) – Biotechnology Post-Graduation Program. Universidade Federal de Pelotas.

The development of reagents for infectious disease diagnosis and prevention is strategic for the scientific and technological advance of the country. Promising results have been obtained with the use of magnetic nanocomposites (MNC) in health for several purposes as separation, purification and detection of cells or biomolecules. In this work, an immunomagnetic separation (IMS) method using carbon and cobalt-based (MNCc), synthesized, and other polystyrene and iron-based (MNCp) commercially available was applied, for the isolation and detection of pathogenic leptospires. The MNCc were synthesized through polymeric precursor method and characterized by scanning electron microscopy/transmission (SEM/TEM), X-ray diffractometry (XRD), infrared spectrometry (FTIR), and immunofluorescence (IF). The MNCc surface was functionalized with carboxylic groups through the incorporation of acrylic acid. MNCc, adsorbed with monoclonal antibodies (MAbs) against pathogenic leptospires, were used in the IMS assays followed by PCR and cell culture was able to detect and isolate the organism. MNCp were used for detecting *Leptospira* spp. in biological fluids from dogs artificially contaminated with leptospires, and clinical samples from dogs positive for leptospirosis. The introduction of IMS, as a step prior to PCR using MNCp, detected a concentration of leptospires ten times smaller when compared to PCR performed directly on artificially contaminated urine and blood samples. Moreover, the IMS performed with MNCp increased PCR sensitivity in clinical samples from dogs positive for leptospirosis. Data from both studies suggest that MNCc and MNCp are important tools for the development of new diagnosis tests.

Keywords: Diagnosis. Cobalt. *Leptospira*.

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1. INTRODUÇÃO GERAL

3 O desenvolvimento de nanocompósitos magnéticos (NCM) vem se destacando na
4 última década visando inúmeras aplicações biotecnológicas (JAIN, 2003; KIM et al., 2009).
5 Entretanto, esta tecnologia tem sido relatada desde os anos 70 e cerca de 35 anos após as
6 primeiras descrições, diversos ensaios usando NCM foram elaborados (HORISBERGER,
7 1976; NAKAMURA; HASHIMOTO; MATSUNAGA, 1991; SCHRODER et al., 1986;
8 NAGARAJAN et al., 2008; PARVEEN; MISRA; SAHOO, 2011). O núcleo magnético e a
9 possibilidade de modificação da superfície proporcionam grande funcionalidade aos NCM e
10 têm atraído a atenção dos grandes centros de pesquisas, já que o alvo magneticamente
11 marcado pode ser detectado diretamente através de um magneto (OLSVIK et al., 1994; JAIN,
12 2008; LIU et al., 2011). NCMs podem ser sintetizados através de várias metodologias e com
13 diversos materiais como metais (ferro, níquel e cobalto), silicatos, polímeros orgânicos ou
14 biológicos, materiais a base de carbono e exibir grande diversidade morfológica tais como
15 formas esféricas e cilíndricas. Além disso, a superfície dos NCM é facilmente manipulada por
16 métodos químicos possibilitando o ancoramento de grupos funcionais incluindo carboxil,
17 amino, hydroxil, hidrazida, clorometil e silanol (NAGARAJAN, 2008). Por esse motivo, uma
18 grande variedade de moléculas pode ser imobilizada com o propósito de capturar o alvo
19 específico (OLSVIK et al., 1994). Devido ao seu pequeno tamanho e alta área superficial,
20 NCM possuem características superiores quando comparado com materiais de dimensões
21 micrométricas.

22 Técnicas convencionais para a preparação de NCM incluem co-precipitação,
23 processamento sol-gel, atomização, liofilização, spray a quente, evaporação-condensação,
24 isolamento de matriz, reações de fase vapor induzidas por laser e aerossóis. Geralmente, a
25 maioria desses métodos, envolve a utilização de equipamentos adequados para cada tipo de
26 material, sofisticados, caros e, além disso, não é possível controlar com precisão a distribuição
27 de poros superficiais e o tamanho dos NCM (PILLAI AND SHAH, 1996). Entretanto,
28 metodologias alternativas vêm sendo desenvolvidas para a síntese de NCM, especialmente
29 formulações que utilizem o elemento cobalto (CARREÑO et al., 2007; PARVEEN; MISRA;
30 SAHOO, 2011). O alto desempenho magnético de compósitos a base desse elemento
31 possibilita a elaboração de ferramentas biotecnológicas como, por exemplo, materiais para
32 ensaios de imunoseparação magnética (BHATT, 2011; PARVEEN; MISRA; SAHOO, 2011).

33 Os avanços e as pesquisas realizadas no desenvolvimento de NCM, especialmente na
34 área da saúde, estão se tornando cada vez mais comuns, (PARVEEN; MISRA; SAHOO,

1 2011) como a elaboração de ensaios para a prevenção de doenças, entrega de drogas,
2 tratamento do câncer, transfecção celular e separação de células ou biomoléculas
3 (MOHANRAJ E CHEN, 2006; PARVEEN; MISRA; SAHOO, 2011). Pesquisas recentes
4 destacam a utilização de NCM para a melhoria na entrega de agentes quimioterápicos com
5 significantes vantagens sobre as atuais metodologias (KIEVIT AND ZHANG 2011). Durante
6 a entrega, os NCM carreadores são injetados na corrente sanguínea e são estrategicamente
7 capturados na região tumoral via aplicação de um campo magnético local. Dessa forma, a
8 droga pode ser liberada no momento adequado através de mudanças fisiológicas (PARVEEN;
9 MISRA; SAHOO, 2011). Além disso, o tratamento de cânceres superficiais por hipertermia
10 também vêm sendo melhorado com o auxílio de NCM, uma vez que é possível concentrar
11 esse material via aplicação de um campo magnético externo no sítio tumoral aumentando a
12 sensibilidade pelas células malignas à radiação e quimioterápicos (SOARES et al., 2010).

13 Como alternativa aos métodos de transfecção celular como a eletroporação,
14 lipofecção e vetores virais, os quais demonstram lenta acumulação e consequentemente baixa
15 concentração do analito na célula alvo, a utilização de NCM demonstra resultados
16 promissores devido à maior eficiência de sedimentação do complexo partículas-tratamento
17 sobre a célula alvo. O aumento obtido nos níveis de transfecção utilizando os NCM pode
18 chegar a até 15 % (YIU et al., 2011).

19 Doenças infecciosas são causadas por micro-organismos patogênicos que podem ser
20 disseminados diretamente ou indiretamente, de uma pessoa para outra ou para animais e vice-
21 versa. Mais de 95% das mortes são causadas devido à falta de medidas eficazes de
22 diagnóstico e tratamento (YAGER et al., 2006). A fim de melhorar a detecção destes
23 patógenos em amostras clínicas e alimentares, os laboratórios necessitam de testes mais
24 rápidos e baratos, como uma alternativa para as atuais metodologias.

25 Nos últimos anos, a imunoseparação magnética (IMS) tem sido citada como uma
26 ferramenta versátil e poderosa para muitas aplicações clínicas (OLSVIK et al., 1994;
27 FERNANDES et al., 2008; MOREIRA et al., 2009). Para a IMS, anticorpos e proteínas
28 específicas podem ser ancorados a superfície dos NCM, os quais são capazes de capturar o
29 micro-organismo ou biomolécula a partir das amostras em estudo (FERNANDES et al., 2008;
30 MOREIRA et al., 2008; GORANSSON et al., 2010; ALBERT et al., 2011). Inúmeras
31 vantagens são atribuídas a IMS como ferramenta laboratorial, tais como a capacidade de
32 reduzir o tempo de isolamento do micro-organismo alvo e as possibilidades de eliminação de
33 contaminantes, já que é possível realizar diversas lavagens com o complexo imunoseparado.
34 Após a IMS, testes laboratoriais podem ser realizados para a detecção do alvo capturado,

1 dentre eles a reação em cadeia da polimerase (PCR) apresenta maior facilidade de execução,
2 rapidez na obtenção de resultados e boa sensibilidade e especificidade quando comparados às
3 metodologias convencionais de cultivo e detecção de micro-organismos (FDA, 1992;
4 TORTORA et al., 2005). Além da aplicação no diagnóstico direto, a IMS pode ser utilizada
5 na otimização do isolamento de agentes patogênicos fastidiosos a partir de fluídos ou tecidos
6 de animais. Esta aplicação pode auxiliar na obtenção de novas cepas, possibilitando análises
7 epidemiológicas, antigênicas e genéticas que contribuiriam para a formulação de novas
8 formas de controle e prevenção de doenças causadas por micro-organismos patogênicos.

9 Devido à importância que a leptospirose representa para a saúde pública mundial,
10 principalmente em países em desenvolvimento (BHARTI et al., 2003; ADLER E
11 MOCTEZUMA, 2010), os ensaios de IMS deste estudo foram realizados com cultivos de
12 leptospiras patogênicas e amostras clínicas de animais positivos para leptospirose.

13 A leptospirose é uma doença infecto-contagiosa causada por mais de 230 sorovares
14 patogênicos pertencentes ao gênero *Leptospira* (ADLER E MOCTEZUMA, 2010). Dentre os
15 ensaios laboratoriais de diagnóstico, a soroaglutinação microscópica (MAT) é considerada o
16 teste referência no Brasil e no mundo (WHO, 2003). No entanto, algumas dificuldades são
17 encontradas para a realização da MAT, tais como a necessidade de uma bateria viva de
18 sorovares de *Leptospira* para a triagem dos soros de humanos e animais suspeitos e um alto
19 grau de reações cruzadas entre diferentes sorovares, onde muitas vezes o resultado revela
20 títulos elevados de anticorpos para sorovares que não são os causadores da enfermidade ou
21 surto (LEVETT, 2003).

22 O isolamento do agente também é realizado para o diagnóstico, porém o crescimento
23 das leptospiras em meios de cultura específicos é lento e pode durar até meses para a
24 caracterização do organismo (WHO, 2003; FAINE et al., 1999). Contudo, o desenvolvimento
25 de metodologias alternativas, como a IMS associada a PCR e ao isolamento, poderia
26 contribuir para o entendimento da doença e a elaboração de testes de diagnóstico mais simples
27 e eficientes, constituindo uma importante estratégia para a prevenção e tratamento da
28 leptospirose. Embora NCM sejam comercialmente disponíveis, ainda existe a necessidade de
29 desenvolver materiais de alta tecnologia em solo brasileiro que apresentem vantagens em
30 relação aos produtos importados tais como NCM com alta estabilidade química e física, fáceis
31 de sintetizar, capacidade de biofuncionalização, propriedades superparamagnéticas e sob
32 custos reduzidos de produção.

1 O objetivo desse trabalho foi produzir NCM de carbono e cobalto usando um método
2 simples de síntese química e avaliar NCM de poliestireno e ferro para o uso em ensaios de
3 IMS visando à detecção e o isolamento de leptospiras patogênicas.

4 A hipótese desse trabalho foi que os NCM sintetizados à base de carbono e cobalto
5 são capazes de ligar covalentemente proteínas e anticorpos; e a IMS realizada com os NCM
6 de poliestireno como passo anterior a PCR aumenta a sensibilidade do teste quando realizada
7 a partir de fluídos biológicos artificialmente contaminados e amostras clínicas de animais com
8 leptospirose.

9 A tese é apresentada na forma de artigos científicos. O artigo 1 relata uma *mini-*
10 *review* com aplicações e inovações biotecnológicas de partículas magnéticas, o qual será
11 submetido ao periódico *Journal of Biosciences*. O artigo 2 relata o desenvolvimento e a
12 caracterização de NCM a base de cobalto e carbono para a aplicação em ensaios de IMS. Esse
13 trabalho será submetido ao periódico *Journal of Nanoparticle Research*. O Artigo 3 relata a
14 aplicação da técnica de IMS utilizando NCM de poliestireno a partir de fluídos biológicos
15 para a detecção de leptospiras patogênicas visando o controle da leptospirose canina. Esse
16 trabalho foi aceito para publicação no periódico *Brazilian Journal of Microbiology*. Todos os
17 artigos estão formatados conforme as exigências dos periódicos científicos em que serão
18 submetidos ou publicados.

19

1 2. ARTIGO 1

2

3 MAGNETIC PARTICLES: A POWERFUL TOOL IN BIOTECHNOLOGY

4

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1 **ABSTRACT**

2 Magnetic particles (MP) varying nanometer to micrometer size can be easily
3 manipulated by magnetic forces and have attracted much attention especially in biological and
4 health area. This article focuses on the potential of MP in biotechnology and current
5 methodologies, describing their advantages, limitations and challenges.

6

7 **Keywords:** Immunoseparation. Diagnosis. Diseases.

8

1 Magnetic particles (MP) varying nanometer to micrometer size have attracted
2 attention as a tool in biotechnology. Several assays based on MP have been developed in
3 which the magnetic field generated by the magnetically labeled targets is captured directly by
4 a sensitive magnetometer, which minimizes the use of expensive laboratory equipments (Jain
5 2008).

6 MP can be artificially (AMP) or biologically (BacMP or magnetosomes)
7 synthesized (Balkwill *et al.* 1980; Matsunaga *et al.* 2006). AMP can be made by several
8 methodologies using diverse materials such as metals (iron, nickel and cobalt), metal oxides,
9 silicates, non-oxide ceramics, polymers organics, carbon materials, organics or biological
10 exhibiting great morphological diversity with shapes such as spheres, cylinders, disks,
11 platelets, hollow spheres and tubes (Nagarajan 2008). The particle's surface is easily
12 manipulated by chemical methods enabling several functional groups to be anchored onto the
13 particle, including carboxyl, amino, hydroxyl, hydrazide, chloromethyl and silanol groups
14 (Gossuin *et al.* 2008; Sun *et al.* 2009; Sun *et al.* 2010; Yuan *et al.* 2011). Therefore, a great
15 variety of molecules can be immobilized on the surface particle with the purpose of capturing
16 the specific target.

17 On the other hand, magnetotactic bacteria can produce intracellular BacMP or
18 magnetosomes of iron oxide, iron sulphides or both that are individually enveloped by a lipid
19 bilayer membrane (Bazylinski *et al.* 1994). Through genetic engineering, functional proteins
20 such as enzymes, antibodies and receptors have been successfully displayed on BacMPs
21 (Arakaki *et al.* 2008). Recently, the biotechnological potential of these platforms has been
22 demonstrated in several assays such as high-performance DNA/RNA recovery,
23 microorganism's detection, magnetic markers and the separation of mononuclear cells from
24 peripheral blood (Yoza *et al.* 2003; Arakaki *et al.* 2008; Fernandes *et al.* 2008; Tanaka *et al.*
25 2008; Maeda *et al.* 2009; Yoshino *et al.* 2010). This article focuses the current methodologies

1 for biotechnological applications of MP, describing their advantages, limitations and
2 challenges.

3 Over 95% of deaths caused by infectious diseases are due to lack of proper diagnosis
4 and treatment (Yager *et al.* 2006). Conventional isolation methods are time-consuming and
5 are not sufficiently sensitive for detection of low concentrations of cells from food and
6 clinical samples (Olsvik *et al.* 1994). Immunomagnetic separation (IMS) has been cited as a
7 versatile diagnostic tool (Fernandes *et al.* 2008; Moreira *et al.* 2009; Deng *et al.* 2011; Fedio
8 *et al.* 2011). For IMS assay, specific proteins can be immobilized on the particles surface,
9 which are able to capture target microorganism or molecule from samples (Gray and Bhunia
10 2005; Urdea *et al.* 2006; Yager *et al.* 2006; Fernandes *et al.* 2008; Moreira *et al.* 2009;
11 Liebana *et al.* 2009; Goransson *et al.* 2010). So, the immune-captured complex can be
12 characterized by routine laboratory tests including plating, biochemical, molecular,
13 immunological, fluorescent or flow cytometry methods (Kim and Ligler 2010; Koktysh *et al.*
14 2011; Leung *et al.* 2011; Zhang and Qi 2011). In IMS procedure, the target is separated from
15 the environment and is concentrated into amounts suitable for identification. Furthermore,
16 growth or PCR inhibitory reagents and contaminants present in the samples are removed
17 (Olsvik *et al.* 1994). Therefore, the association of the IMS step with current methodologies
18 would enhance the degree of sensitivity, automation and reproducibility, which are parameters
19 important to clinical applications.

20 MP have been applied in healthcare to improve delivery of chemotherapeutic agents
21 in cancer treatment with the goal of minimizing toxic effects on healthy tissues with a
22 significant advantage over standard chemotherapies by increasing the drug delivery
23 specifically to the tumor site (Yezhelyev *et al.* 2006; Cherry *et al.* 2010; Kievit and Zhang
24 2011). In magnetic drug targeting, magnetic carrier particles with surface-bound drugs are
25 injected into the vascular systems that are then captured at the tumor via a locally applied

1 magnetic field. The surface-bound drugs can be released from the drug carriers by changing
2 the physiological conditions, and are then taken up by the affected cells (McBain *et al.* 2008;
3 Parveen *et al.* 2011). Particles must remain in circulation long enough for tumor
4 accumulation. However, they are prone to clearance by the mononuclear phagocyte system.
5 The most common strategy has been grafting PEG or other macromolecules such as
6 polysaccharides onto the particle surface (Wang *et al.* 2011), preventing protein adsorption,
7 interactions among particles and interactions with immune cells (Peracchia *et al.* 1998).

8 Hyperthermia is an old concept and it has long been established as an option in the
9 treatment of cancer, mainly in superficial cancers. More recently the concept of intracellular
10 hyperthermia emerged wherein magnetic particles are concentrated at the tumor site and
11 heated remotely using an applied magnetic field to achieve hyperthermic temperatures. It is
12 also well established that by exposing cancer tissue to elevated temperatures, the viability of
13 the cells is reduced and an enhancement of their sensitivity to radiation and chemotherapy is
14 observed (Soares *et al.* 2010).

15 Screening for circulating tumor cells in blood has been an object of interest for
16 evidence of progressive disease, status of disease activity and for early diagnosis of cancer
17 (Hoshino *et al.* 2011). It is known that several types of cancers over express specific proteins
18 on the tumor cell surface which enter the blood stream and serve as clinical biomarkers for
19 neoplastic lesions (Ferrari 2005). For highly specific separation of tumor cells, the
20 introduction of immune separation-based detection is desirable, in which antibodies for
21 tumor-specific markers are utilized to label target cells (Hoshino *et al.* 2011; Kievit and
22 Zhang 2011).

23 The transfection of genes into eukaryotic cells has become an important technique
24 for analysis of gene function, production of recombinant gene products and gene therapy. MP
25 are being increasingly used in cell sorting and transfection (Yang *et al.* 2008) as an alternative

1 method over use of pure plasmids, electroporation, receptor-mediated gene transfer, particle
2 guns, viral vectors and lipofection (Hoelker *et al.* 2007; Yang *et al.* 2008). However, each
3 methodology has benefits and limitations, and to date there is still no ideal system for gene
4 transfer (Hoelker *et al.* 2007). Among these limitations, the slow accumulation and
5 consequently low concentration of analyte in the target cell have been identified as simple but
6 strong barriers to effective gene transfection (Luo and Saltzman 2000). Magnetofection is a
7 new method for gene transfer that has shown promising results. This assay involves the use of
8 magnetic force and plasmid DNA/magnetic bead complexes, and it has been developed for
9 enhancing delivery of gene vectors to target cells (Gersting *et al.* 2004; Kadota *et al.* 2005). In
10 the magnetofection procedure, the efficient sedimentation of the target-magnetic particles
11 complex generated by an external magnetic field provides the largest fraction t of target
12 (cells) within a few minutes of incubation and may increase levels of transfection up to 15%
13 (Plank *et al.* 2003; Yiu *et al.* 2011). In addition, cationic magnetic particles mediate cell
14 binding which is followed by internalization (Scherer *et al.* 2002).

15 Scaffolds play a pivotal role in tissue regeneration, which provides specific macro
16 and micro structure to modify the biological and biomechanical reaction of the cells during
17 the healing process (Sangsanoh *et al.* 2007; Schnell *et al.* 2007). Cell adhesion onto scaffolds
18 is the first fundamental step in bone regeneration, which will greatly influence the
19 morphology and capacity of cell proliferation and differentiation (Ma *et al.* 2005). The
20 electrospinning, aided by MP, is a technique that has been used for the synthesizing of
21 nanofibrous scaffolds and is proving to be a promising material for tissue regeneration. The
22 key factor for use of this technique lies in the possibility of generating a surface tension by
23 using MP and external voltage field during the biomaterial polymerization that facilitates the
24 scaffolds formation. Electrospun nanofibrous membranes are considered to be of great
25 potential in the field of tissue regeneration, since they can closely mimic the extracellular

1 matrix architecture. The electrospinning process also provides operational flexibility for
2 incorporating multiple components into nanofiber, such as metal nanoparticles (Pt, Ag, Au)
3 and inorganic compound nanoparticles (TiO_2 , SiO_2). In addition, this process has helped in
4 osteoinduction promoting significantly higher proliferation rate and faster differentiation of
5 osteoblast cells (Meng *et al.* 2010).

6 Although the potential benefits of MP are considerable, there is a definite need to
7 identify any potential negative responses in ecosystems and humans (He *et al.* 2011).
8 Furthermore, drawbacks can be found during the synthesis process causing adverse effects for
9 their use (Kwon *et al.* 2008; Morimoto *et al.* 2010). A recent study with *Escherichia coli*
10 organism demonstrates that iron oxide magnetic particles induced genomic mutations leading
11 to morphological changes (He *et al.* 2011). In addition, the effect of static magnetic fields that
12 can lead to aggregation and cytotoxicity in biological system. So, different approaches to
13 synthesis of MP are essentials to increase the biocompatibility these materials (Bae *et al.*
14 2011).

15 MP without any surface coatings can generate hydrophobic surfaces with a large
16 surface area to volume ratio, which leads to agglomeration and formation of large clusters,
17 resulting in increased particle size. This inherent aggregation behaviour of particles is a
18 crucial limiting factor that reduces the quality of the material (Gupta and Gupta 2005).
19 Aiming to avoid the particles potential toxic effects, the toxicological and chemical
20 characterization of new composites is necessary (Oberdorster *et al.* 2005). In addition,
21 immune system defense mechanisms studies against MP could elucidate and minimize
22 adverse effects in animal and human health.

23 In conclusion, MP has been cited as a powerful tool in biological and health areas.
24 Despite problems related to their synthesis and toxicity, this advance in technology is a new
25 approach in the detection of microorganisms and molecules in food and clinical samples.

1 **Acknowledgments**

2

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22

3. ARTIGO 2

SYNTHESIS AND BIOFUNCTIONAL VALIDATION OF COBALT MAGNETIC NANOPARTICLES EMBEDDED IN CARBON MATRIX

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1 **ABSTRACT**

2

3 Carbon nanostructures and nanocomposites display versatile allotropic morphologies,
4 physico-chemical properties and have a wide range of applications in mechanics, electronics,
5 biotechnology, structural material, chemical processing and energy management. In this work
6 we report the synthesis, characterization and biotechnological application of cobalt magnetic
7 nanoparticles embedded in carbon structure (Co/C-MN). A single-step chemical process was
8 used in the synthesis of the Co/C-MN. The Co/C-MN has presented superparamagnetic
9 behavior at room temperature an essential property for immunoseparation assays carried out
10 here. To stimulate covalent interactions between proteins and Co/C-MN, this nanocomposite
11 was functionalized with acrylic acid (AA). We have showed the bonding of different proteins
12 onto Co/C-AA surface by using immunofluorescence assay. A Co/C-AA coated with
13 monoclonal antibody anti-pathogenic *Leptospira* spp. was able to capture leptospires,
14 suggesting that it could be useful in immunoseparation assays.

15

16 **Keywords:** Immunoseparation assays. Pechini method. *Leptospira*.

17

1 **1. Introduction**

2 Carbon nanostructures and nanocomposites (NC) display versatile allotropic
3 morphologies as also physico-chemical properties and are widely used in mechanics,
4 biotechnology, electronics, structural materials, chemical processing and energy management
5 (Chang et al. 2003; Carreño et al. 2007). Among these properties, much attention has been
6 paid to nanostructured magnetic systems due to their magnetic behavior, which is related to
7 particle size and the type of support matrix used. NC may provide an appropriate morphology
8 derived from of type porous (microporous or mesoporous) surface, that allow host inorganic
9 particles and organic substance , potential factor necessary to advance applications (McHenry
10 et al. 1994).

11 Superparamagnetism has been demonstrated in Fe, Ni and Co ferromagnetic
12 nanoparticles embedded in an amorphous matrix (Childress and Chien 1991; McHenry et al.
13 1994). Magnetic nanoparticles (MN) have been extensively studied in biomedical applications
14 including magnetic resonance imaging (MRI) contrast agents, magnetic targeting of drug
15 delivering vehicles and magnetic separation of DNA, proteins and cells (Çakmak et al. 2009).

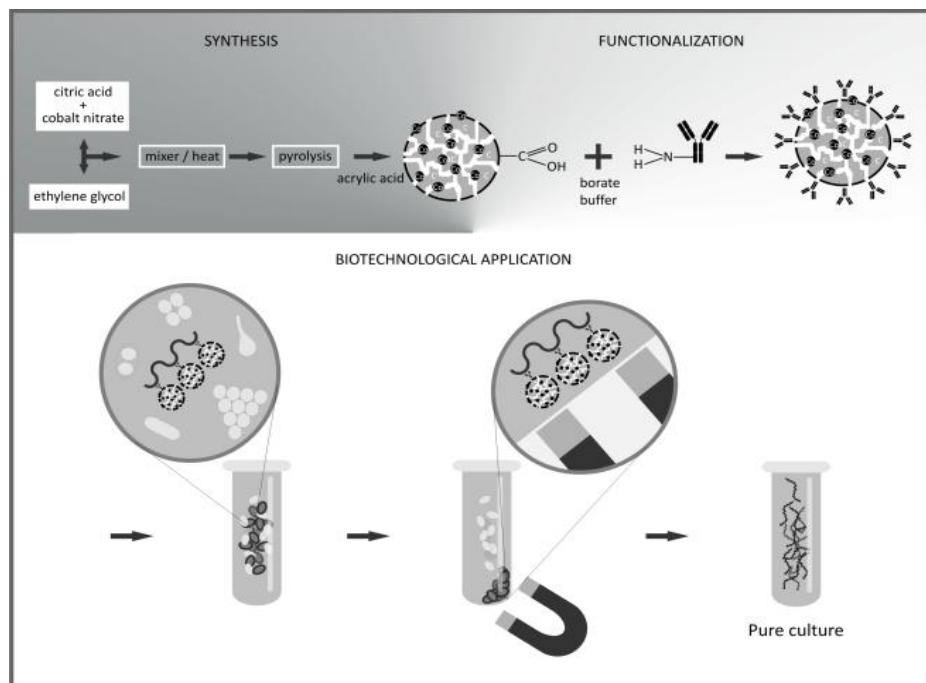
16 Selection and assembly of materials are the main issues in the development of
17 diagnostic assays, vaccines and epidemiological studies to control and prevention of diseases
18 caused by pathogenic micro-organisms. (Gray and Bhunia 2005; Kim et al. 2010).
19 Immunomagnetic separation (IMS) aided by proteins and antibodies is a technique that has
20 been used for detection and isolation of specific organisms. After IMS, it is possible to
21 cultivate and identify the target organism by traditional biochemical, immunological or
22 molecular methods (Olsvik et al. 1994; Fernandes et al. 2008). Although magnetic particles
23 are commercially available, there is still need to produce materials with improved properties,
24 e.g. easy preparation, easy surface modification, low cost and superparamagnetic property.
25 Conventional techniques for the preparation NC include bulk precipitation, sol-gel processing,

1 spray-drying, freeze-drying, hot-spraying, evaporation-condensation, matrix isolation, laser-
 2 induced vapor phase reactions and aerosols. Generally, in most types of NC prepared by these
 3 methods, it is usually not possible to control precisely the size and size distribution of the NC
 4 (Palli and Sohah, 1996). In this context, the aim of this study was to synthesize cobalt/carbon
 5 nanocomposite (Co/C-NC) by a single-step chemical process, anchor specific proteins onto
 6 Co/CNC surface and evaluate them in IMS assay for the capture of pathogenic leptospires.

7

8 2. Materials and methods

9



10

11 *Figure 1.* General schematic diagram of nanocomposite synthesis by polymeric precursor
 12 method and immunomagnetic separation of pathogenic leptospires.

13

14 2.1. Synthesis of the Co/C-nanocomposite

15 A single-step chemical process was used in the synthesis of the cobalt/carbon
 16 nanocomposite (Co/C-NC), figure 1. The synthesis procedure consists in dissolution of citric
 17 acid (CA; Synth, USA) and the cobalt salt, $\text{Co}(\text{NO}_3)_2 \cdot 6\text{H}_2\text{O}$, using a CA:Co molar ratio of

1 3:1 in water (Pechini, 1967). This mixture was homogenized for 15 min at room temperature
2 and polymerization was initiated by adding ethylene glycol at a mass ratio of 40:60 in relation
3 to the CA, at approximately 80 °C. The final composites were obtained by a two step
4 pyrolysis of the polymeric intermediate. The first step (2 h, 250 °C) promoted the breakage of
5 the organic parcel of the polymeric intermediate. The powder was submitted to a second heat
6 treatment, performed in a N₂ atmosphere ranging between 600 °C and 800 °C, to produce the
7 cobalt magnetic nanoparticles (Co/C-MN). The CO/CO₂ atmosphere resulting from the
8 pyrolysis of the organic material promoted the reduction of the Co salt without using H₂ as a
9 reducing agent (Leite et al. 2002).

10 2.2. *Characterization of the Co/C-MN*

11 Using SiO₂ as an external standard the crystalline phases and the cell volume were
12 determined by examining X-ray diffractometry (XRD) patterns which were obtained with a
13 Shimadzu XRD-6000 diffractometer with Cu K λ radiation ($\lambda=1.5406$ Å). Morphological
14 characterizations were performed by scanning electron microscopy (SEM) and transmission
15 electron microscopy (TEM) using a Philips, model CM200 equipment.

16 Samples were characterized by N₂ adsorption/desorption isotherms obtained at the
17 temperature of liquid nitrogen in an automated physisorption instrument (Autosorb-1C,
18 Quantachrome Instruments). Prior to the analysis, the samples were degassed in a vacuum at
19 300°C for 2-3 h. Specific surface areas were calculated according to the Brunauer–Emmett–
20 Teller (BET) (Brunauer et al. 1938) method, and the pore size distributions were obtained
21 according to the Barret-Joyner-Halenda (BJH) method from the adsorption branch data.

22 2.3. *Co/C-MN surface modification*

23 The Co/C-MN was functionalized using a physical coating method. The particle
24 surface was coated with acrylic acid through a polymerization reaction. The Co/C-MN
25 particles were dispersed in acrylic acid, 2.9 mol.L⁻¹ at approximately 100 °C. To improve the

1 coating, particle dispersion was increased by incubation in an ultrasonic bath for 2 h followed
2 by drying at 50 °C. These coated MN were defined as Co/C-AA. For a comparative study,
3 other concentrations (1 mol.L⁻¹ and 0.5 mol.L⁻¹) of acrylic acid were also evaluated.

4 *2.4. Characterization of the Co/C-AA*

5 The samples functionalized and not functionalized were analyzed by Fourier
6 Transform Infrared Spectroscopy (FT-IR, Varian, model 640-IR) to detect the presence of the
7 carboxylic groups responsible for the covalent bonds between the Co/C-AA surface and
8 proteins. In addition, magnetic measurements (Quantum Design, model PPMS) were carried
9 out to verify the behavior of the NC in an external magnetic field. The zeta potential of the
10 Co/C-AA was determined by a Zetasizer Nano ZS (Malvern Instruments, Malvern, U.K.)
11 instrument at ambient temperature. The concentration of Co/C-AA suspension was 5 mg.mL⁻¹
12 using the samples dispersed on phosphate buffer saline with pH 7.4.

13 *2.5. Preparation of biofunctional Co/C-AA*

14 Heating at 80 °C for 15 min was performed to reduce microbial contaminants prior to
15 starting the preparation of the biofunctional Co/C-AA. Immobilization of proteins was carried
16 out as previously described (Çakmak et al. 2009). Briefly, recombinant LipL32, the most
17 abundant surface lipoprotein on the outer membrane of pathogenic *Leptospira* spp. (Haake et
18 al. 2000), anti-LipL32 monoclonal antibody (MAb) (Fernandes et al. 2007) and protein A
19 were attached to the Co/C-AA surface in 0.05 M borate buffer (pH 9.5). All proteins were
20 used at high concentrations (1.2 mg.mL⁻¹) for nanoparticle surface saturation. To detect the
21 bound LipL32, anti-LipL32 MAb or protein A onto Co/C-AA surface, anti-LipL32 MAb
22 and/or goat-anti mouse fluorescent isothiocyanate (FITC) conjugate (Sigma) were used.
23 Protein-Co/C-AA complexes were observed by immunofluorescence microscopy (Olympus
24 BX 51) at an excitation wavelength of 450 nm. Control reactions were performed using an

1 anti-internalin A MAb specific for *Listeria monocytogenes* and phosphate buffer saline with
2 0.05% of Tween-20.

3 **2.6. Biofunctional assay of the Co/C-AA**

4 In order to assess the biotechnological application of these surface-modified MN, an
5 IMS assay using *L. interrogans* serovar Canicola Hond Utrecht IV strain was carried out as
6 previously described (Fernandes et al. 2008). Briefly, Co/C-AA attached to the anti-LipL32
7 MAb were added to a liquid culture of the *L. interrogans* strain. The biotechnological
8 application of IMS is represented in figure 1. To perform the experiments an
9 immunomagnetic separator MPC-S (Invitrogen, CA, USA) was used according to the
10 manufacturer's instructions. The presence of DNA from the immunomagnetic-captured
11 leptospires was confirmed by PCR using primers specific for *lipL32* gene as previously
12 described (Haake et al. 2000). In addition, captured leptospires were inoculated into
13 Ellinghausen-McCullough-Johnson-Harris liquid medium (EMJH, Difco-USA). To evaluate
14 the nonspecific interaction between the Co/C-AA and the leptospires, a control reaction was
15 performed using the Co/C-AA without the anti-LipL32 MAb. The cultures were examined
16 daily for contamination and evidence of growth.

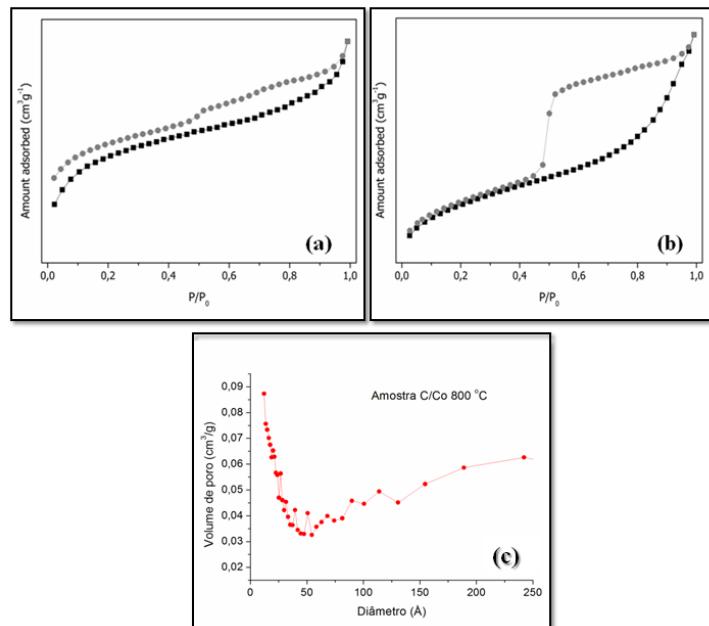
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18 **3. Results and discussion**

19

20 Figure 2 shows the N2 adsorption/desorption isotherms obtained from the carbon
21 nanocomposite. Figure 2a, according to the nomenclature of International Union of Pure and
22 Applied Chemistry (IUPAC), shows isotherms with a loop similar to the type H4, that is often
23 associated with narrow slit-like pores, but in this case the type I isotherm character is
24 indicative of microporosity. Figures 2b illustrate an isotherm as a type IV isotherm with a
25 type H2 hysteresis, usually associated with capillary condensation in mesopore structures.

1 Figures 2c demonstrate the results obtained with BJH method which indicated the distribution
 2 homogeneous of pore onto Co/C-AA surface.



3
 4 *Figure 2.* (a) and (c) nitrogen adsorption/desorption isotherms obtained by BET method for
 5 Co/C-AA samples pyrolyzed at different 600 °C and 800 °C, respectively. The dark symbols
 6 refer to the adsorption branch and gray symbols to the desorption branch. (c) pore size
 7 distribution obtained by BJH method for Co/C-AA calcined at 800 °C.

8
 9 Table 1 summarizes the surface specific area and average pore diameter. The results
 10 show a significant increase in the surface area and average pore diameter of samples with the
 11 rise in pyrolysis temperature from 600 °C to 800 °C. In addition, the results for the Co/C-MN
 12 coated with acrylic acid show a significant decrease in the sample's surface specific area with
 13 the rise in pyrolysis temperature from 600 °C to 800 °C and acrylic coated process, changing
 14 from microporous to mesoporous was also observed, respectively, suggesting that residual
 15 carbon is an important factor in the material's morphological properties and during the
 16 process of fixing of acrylic acid on the surface of Co/C-MN.

17

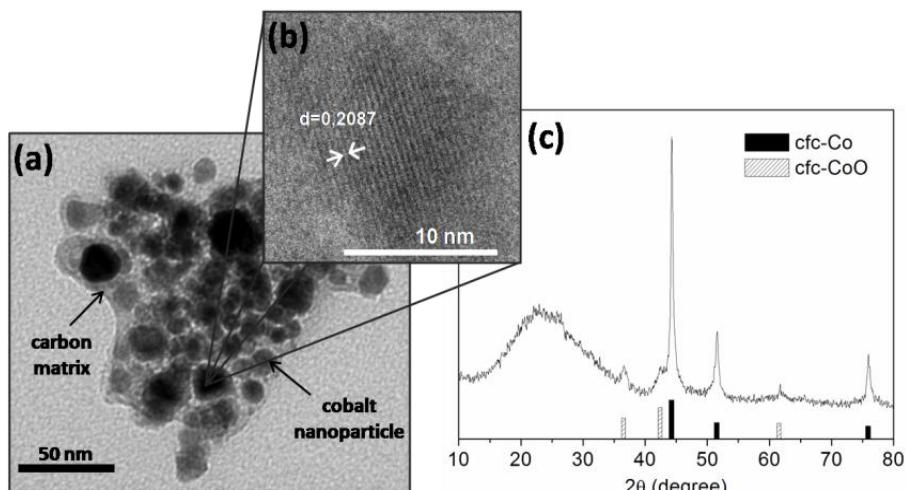
1 *Table 1.* Surface specific area and average pore diameter of cobalt magnetic nanoparticles
 2 embedded in carbon structure.

Samples	Surface specific area (m ² .g ⁻¹)	Average pore diameter (Å)
Co600	134	29
Co800	116	37
Co800AA	2	167

3

4 Figure 3a shows a HRTEM image of the Co/C-AA with a diameter between 10 and 20
 5 nm, embedded in a shell of the carbonaceous matrix. In Figure 3b it is possible to observe the
 6 atomic planes from cfc-Co (JCPDS 89-4307), with interplanar spacing $d_{(111)} = 0.2087$ nm
 7 (Pola et al. 2010). Sharp peaks showed in XRD pattern confirmed the presence of cfc-Co,
 8 figure 3c. In addition, a region characteristic of amorphous carbon preserved from chemical
 9 synthesis was observed. Furthermore to the cfc-Co peaks, small intense peaks due to the
 10 presence of cobalt oxide from the first pyrolysis step were also observed. However, this did
 11 not affect the final application negatively due to the small amount of material present. Cobalt
 12 content in Co/C-AA sample was measured by inductively coupled plasma optical emission
 13 spectrometry (ICP OES), which showed about 42.3% cobalt.

14



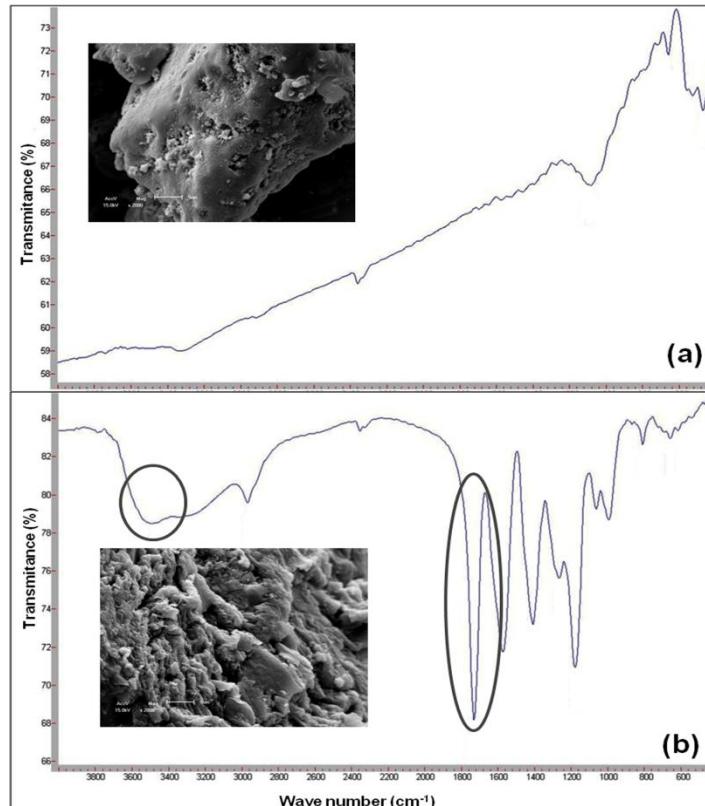
15

1 *Figure 3.* (a) and (b) show HRTEM images and (c) XRD pattern of cobalt/carbon calcined at
2 800 °C, in N₂ atmosphere.

3

4 As expected, there were no significant peaks in the FT-IR spectrum of the Co/C-AA
5 (figure 4a). However, analysis of the Co/C-AA identified three peaks, located at 1732 cm⁻¹,
6 1411 cm⁻¹ and 3493 cm⁻¹ (figure 4b). These peaks were attributed to stretching of the C=O, C-
7 O and O-H bonds, respectively. There was another peak due to C=C stretching at 1574 cm⁻¹
8 and other bands of stretching out-of-plane bending and secondary absorptions (Liu et al.
9 2009; Zheng et al. 2005). These results suggested that the Co/C-AA surface was successfully
10 coated with a polymeric layer that contained carboxyl groups. Furthermore, on comparing the
11 MEV images, there were differences in the composite before and after functionalization
12 (figure 4). This observation suggested that the acrylic acid was polymerized and that the
13 granules of the Co/C-AA were maintained inside its polymer structure. The presence of
14 carboxyl groups, as shown by infrared analysis, enabled interaction with biomolecules,
15 mainly through the amino groups.

16

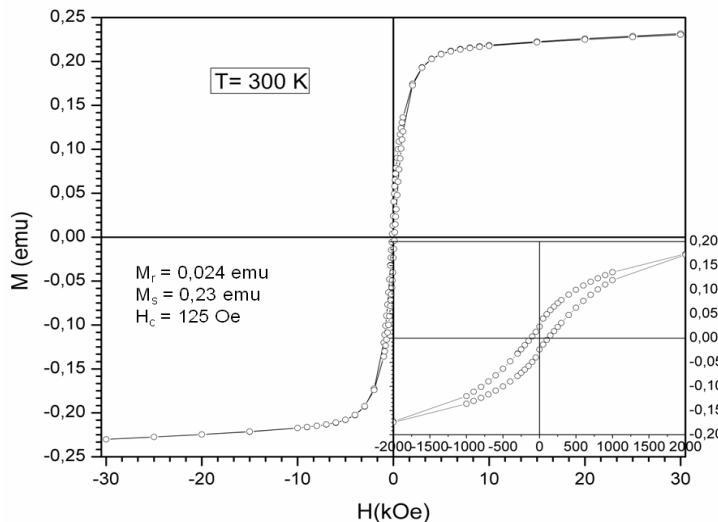


1 **Figure 4.** FT-IR spectrum and MEV image (2000 x) of cobalt/carbon nanoparticles (a) not
 2 functionalized and (b) functionalized with acrylic acid.

4

5 The results of the magnetic measurements of the Co/C-AA sample are showed in
 6 figure 5. The magnetic behavior at 300 K is indicated by the saturation magnetization (M_s),
 7 remanent magnetization (M_r) and coercive field (H_c). Magnetization ratio (M_r/M_s) and H_c
 8 values different from zero at room temperature indicate that there is a residual magnetic
 9 moment of the nanoparticles (Cheng et al. 2005). The value of the magnetization ratio
 10 presented for Co/C-AA was low (0.104), suggesting superparamagnetic behavior at room
 11 temperature (Sajitha et al. 2004). In addition, the Co/C-AA developed in this work presented
 12 M_r/M_s ratio of $H_c = 125$ Oe, consistent with values reported by other superparamagnetic
 13 nanoparticles. These nanoparticles have potential in several biotechnological applications,
 14 such as immunoassays, magnetic resonance imaging, magnetic cell separation, magnetic
 15 oligonucleotide and nucleic acid separation (Cheng et al. 2005; Yu and Qiu 2008).

1



2

3 *Figure 5. Magnetization curve for Co/C-AA sample at 300 K.*

4

5 For a comparative study, other concentrations of acrylic acid to functionalize
 6 nanocomposites were also formulated, but these samples did not show good applicability and
 7 stability. Illustrated by zeta potential (table 2), which expresses the colloidal stability by
 8 surface charge of particles, it can be said that stability increased with the concentration of
 9 acrylic acid in the modification of the particles, since the zeta potential values became more
 10 negative when we increased the concentration of acid. Demir-Cakan et al. (2009) explain that
 11 this can be due to the fact that zeta potential is a surface technique and although most of the
 12 acidic functionalities are located on the surface for carbonaceous materials and suggest that
 13 presumably some of the carboxylic groups for the acrylic acid coated samples are also located
 14 within the carbon matrix.

15 Additional information found in literature presented by Jans and coauthors (Jans et al.
 16 2010) synthesized nanoparticles stabilized by poly (acrylic acid) with zeta potential near -50
 17 mV, while at pH 7. This potential is very negative because there are many deprotonated

1 carboxylic groups. The same is presented in our composites coated with acrylic acid, but the
 2 carboxyl groups are more protonated, maintaining the zeta potential close to -20 mV.

3

4 *Table 2.* Zeta potential values for Co/C-MN recovered with different acrylic acid
 5 concentrations.

Acrylic acid (mol.L ⁻¹)	Zeta potential (mV)
Control (No acrylic acid)	-24.9
0.5	-8.31
1	-3,5
2.9	-19,5

6

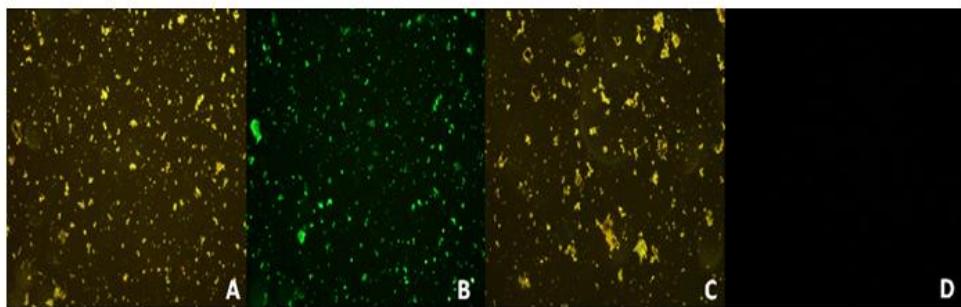
7 Mohapatra and Pramanik (Mohapatra and Pramanik 2011) studied the behavior of
 8 phosphoric acid coupling agents on Co/C-AA in an aqueous medium and showed that
 9 functional nanoparticles were highly stable and presented potential for use in biomedical
 10 applications. Çakmak and co-workers (Çakmak et al. 2009) produced monodisperse poly
 11 (glycidyl methacrylate) microspheres by dispersion polymerization that covalently
 12 immobilized protein A. Similar results have been obtained comparing the method of
 13 functionalization presented in this article with those described in the literature (Çakmak et al.
 14 2009; Mohapatra and Pramanik 2011), however, our process is simpler, with less steps in the
 15 synthesis, since it is possible to disperse directly the Co/C-MN into solution of acrylic acid. In
 16 addition, we avoid the steps of synthesis from organic precursor for carboxyl groups or
 17 activation of already existing groups and also a route using the functionalization system of
 18 high control, such as temperature, pH, among others.

19 We also used a simple method for the immobilization of the proteins onto the Co/C-
 20 AA surface, based on peptide ligation promoted by borate buffer (Çakmak et al. 2009). The
 21 maximum immobilization capacity from LipL32, anti-LipL32 MAb and protein A was found
 22 to be 0.9 mg.mL⁻¹, 0.7 mg.mL⁻¹ e 0.8 mg.mL⁻¹, respectively. Immunofluorescence assays

1 were used to confirm the immobilization effects. Mixes of Co/C-AA and proteins incubated
2 with borate buffer produced fluorescent complexes, unlike those incubated with phosphate
3 buffer saline (figure 6). These results suggest that proteins were efficiently ligated to Co/C-
4 AA surface.

5

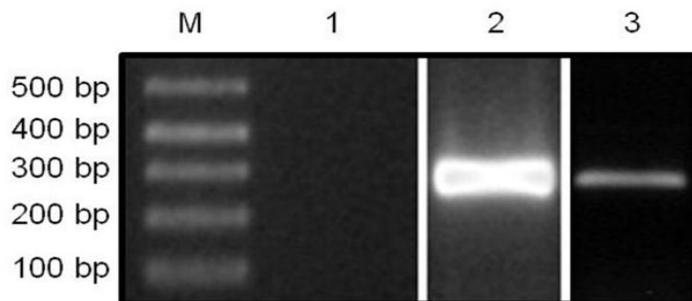
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7 *Figure 6.* Immunofluorescence assay demonstrating the MAb anti-LipL32 attached to Co/C-
8 AA. Panel “A” and “C”, nanoparticles in dark field; Panel “B”, anti-LipL32 MAb-Co/C-AA
9 complex detected with goat anti-mouse fluorescent isothiocyanate (FITC) conjugate (Sigma);
10 Panel “D”, negative control using phosphate buffer saline with 0.05% of Tween-20 as ligation
11 buffer. Labeling was visualized by fluorescence microscopy (Olympus BX 51) with excitation
12 wavelength of 450 nm with a 100× objective.

13

14 Biofunctional assay demonstrated the capacity of the Co/C-AA coated with anti-
15 LipL32 MAb to capture leptospires. Conversely, the Co/C-AA without the anti-LipL32 MAb
16 was not able to capture leptospires (figure 7). These results were similar using commercial
17 magnetic particles of iron and polystyrene for detection of pathogenic leptospires and
18 *Salmonella* Typhimurium organisms (Fernandes et al. 2008; Moreira et al. 2009). In addition,
19 the growth of leptospires after immunoseparation followed by subculture was observed,
20 suggesting that Co/C-AA could help in obtaining new leptospira isolates and others
21 pathogenic microorganisms.



1

2 *Figure 7.* Agarose gel electrophoresis of IMS-PCR products from leptospiral strain culture
 3 showing the detection of *lipL32* gene (264 bp). M, 1kb Plus DNA Ladder; 1, Co/C-AA
 4 without anti-LipL32 MAb; 2, Positive control reaction (genomic DNA of *Leptospira* sp.); 3,
 5 Co/C-AA with anti-LipL32 MAb on the surface

6

7 **4. Conclusions**

8 The cobalt magnetic nanoparticles embedded in carbon matrix (Co/C-AA) produced
 9 in this article were prepared successfully using a single chemical one step method which
 10 varying 20 nm to 50 nm size. The effective incorporation of acrylic acid surface on carbon
 11 mesoporous material was a decisive factor in bonding specific proteins and developing a
 12 biofunctional material for the isolation of microorganisms and detection approaches.

13 The Co/C-AA synthesized here suggests an important material in biotechnological
 14 applications.

15

16 **Acknowledgments**

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 18 CAPES/Nanobiotecnologia for financial support, and Prof. Adilson Jesus Aparecido de
 19 Oliveira by experimental contribution.

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26

1 **4. ARTIGO 3**2
3 **DIAGNOSIS OF CANINE LEPTOSPIROSIS USING AN IMMUNOMAGNETIC**
4 **SEPARATION-PCR METHOD**5
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20

1 **ABSTRACT**

2 Diagnosis of leptospirosis by PCR is hampered due to the presence of substances on
3 biological fluids. Here, we report an immunomagnetic separation step prior to PCR which
4 improved the detection of *Leptospira* spp. in blood and urine samples from dogs. It resulted in
5 a significant improvement on sensitivity for diagnosis of canine leptospirosis.

6

7 **Keywords:** Canine leptospirosis, IMS-PCR, LipL32.

8

9 Leptospirosis is a zoonosis of ubiquitous distribution, caused by infection with
10 pathogenic *Leptospira* spp., which occurs in many animal species and humans (1). Dogs may
11 be exposed to leptospires in the environment by contact with urine of an infected host,
12 contaminated water or moist soil, where the bacteria may survive for several months (5, 12).
13 In the last years, several assays have been proposed for confirmation of canine leptospirosis,
14 including serology, polymerase chain reaction (PCR), fluorescent antibody testing of urine or
15 tissue samples, or organism isolation (8).

16 The recommended laboratory diagnostic test, microscopic agglutination test (MAT),
17 is based on detection of antibodies against *Leptospira* spp. in dog sera; however, pathogen-
18 specific antibodies may remain in the blood stream for a long period, even after recovering
19 from disease. Besides serology, demonstration of leptospires by culture of blood, tissues or
20 urine is definitive; it also identifies the infecting leptospire (7).

21 PCR assay is highly sensitive, but the presence of PCR inhibitory substances on
22 biological fluids can prevent amplification, resulting in false negative (10). Recent studies
23 report the immunomagnetic separation (IMS) technique prior to PCR assay as an approach to
24 reduce the effect of inhibitory substances present in biological fluids and food samples (2, 3,
25 4, 6, 7, 9, 14, 15). For diagnosis of leptospirosis, the IMS-PCR approach was reported to

1 detect *Leptospira* spp. in bovine urine (15) and in human biological fluids (6). In order to
2 improve PCR sensitivity and specificity, we developed a novel IMS-PCR approach by using
3 both magnetic beads in house coated with a monoclonal antibody (mAb) and specific PCR
4 primers for pathogenic *Leptospira* spp. (6, 9). Blood and urine samples were obtained from
5 dogs suspected of having leptospirosis (n=5) at the Veterinary Hospital/ Universidade Federal
6 de Pelotas, Brazil. Blood samples were centrifuged at 2,000 x g for 5 min, the supernatant was
7 collected, and one drop was observed under microscope to investigate the presence of
8 spirochetes by darkfield microscopy (DFM) on an Olympus BX 51 microscope. Control
9 samples were obtained from healthy dogs (n=5) negative by MAT. The MAT was performed
10 according to Faine *et al.* (5), using reference strains of 19 different leptospiral serovars.
11 Reciprocal agglutination titres of greater than or equal to 1:100 were considered positive
12 reactions.

13 For PCR assay, blood sera and urine samples were centrifuged at 15,000 x g for 10
14 min. The cells were washed with sterile 0.01 M phosphate-buffered saline (PBS, pH 7.2) and
15 the DNA was extracted by heating at 95 °C for 15 min in 50 µL of lysis solution (1:1 of
16 0.125% SDS and 0.05 M NaOH). In experiments in which lysis followed IMS, 20 µL of the
17 lysis solution were directly added to immune separated products in microtubes and then
18 heated at 95 °C for 15 min. Primers *lipL32* F: 5' CGCTTGTGGTGCTTCGGTGGT 3' and
19 *lipL32* R: 5' CTCACCGATTCGCCTGTTGGG 3' were used, resulting in a 264 bp
20 amplicon of the *lipL32* coding region (9). Amplification was carried out in a Peltier Thermal
21 Cycler PTC-100® (Bio-Rad) with 1 cycle at 94 °C for 5 min, 35 cycles at 94 °C for 1 min, 55
22 °C for 1 min, 72 °C for 1 min, followed by an extension for 7 min at 72 °C at the end of the
23 final cycle. Aliquots were analyzed by electrophoresis in 1% agarose gel with ethidium
24 bromide and visualized under UV transillumination. A specific PCR internal amplification
25 control (IAC) was used in all assays, which consists of a DNA fragment containing 501 bp

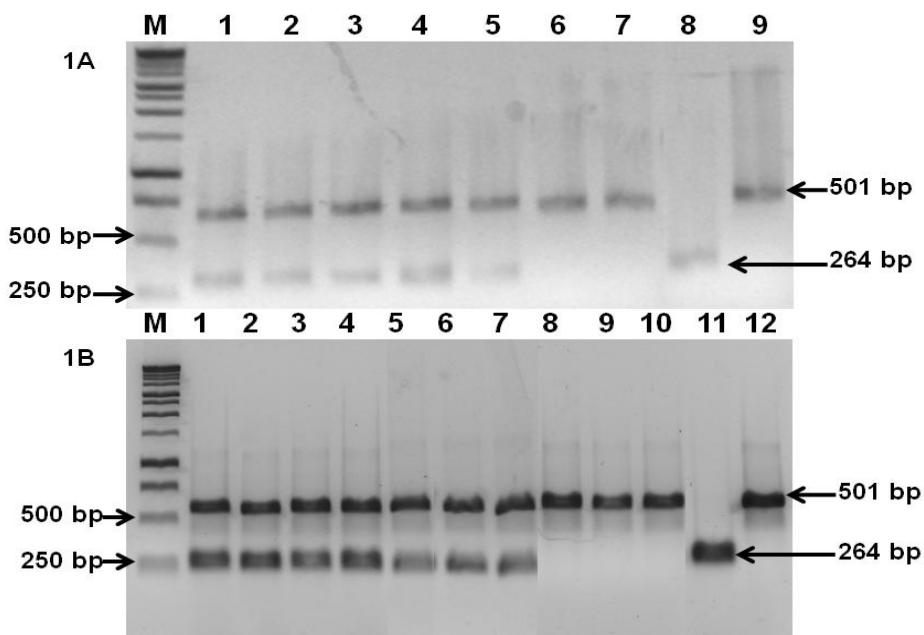
1 not related to *Leptospira* spp., flanked by target sequences of *lipL32* primers (6). The IAC
2 concentration was estimated spectrophotometrically at 260 nm and the optimal concentration
3 for use in the *lipL32* PCR was determined by titration, and the lowest reproducible
4 concentration was determined using decimal dilutions of IAC (50 to 0.05 pg) as template
5 DNA in a PCR with *lipL32* primers. PCR and IAC-PCR were performed using a single pair of
6 *lipL32* specific primers.

7 Determination of the minimal concentration of DNA and number of leptospiral cells
8 required to result in amplification of the *lipL32* gene sequence by PCR was carried out
9 according to Fernandes *et al.* (6). Briefly, genomic DNA from *L. interrogans* was diluted with
10 sterile 10 mM Tris-HCl, 1 mM EDTA (TE, pH 8.0) to concentrations ranging from 20 to 1
11 pg/µL, and pellets from control samples artificially contaminated with *Leptospira interrogans*
12 serovar Canicola strain Hond Utrecht IV at concentrations ranging from 10^8 to 10^0 cells per
13 mL. Then, the pellets from each DNA concentration and bacterial dilution were washed with
14 PBS and suspended in 50 µL of lysis buffer for DNA extraction. DNA extracted from
15 saprophytic *L. biflexa* serovar patoc Patoc I or *E. coli* were used as negative controls. These
16 experiments were repeated three times.

17 The IMS-PCR was performed with protein A-magnetic beads (Bangs Laboratories
18 Inc, Fishers, IN, USA) adsorbed with a mAb against leptospira LipL32 protein according to
19 the manufacturer's instructions. The mAb used in this work is specific to pathogenic
20 leptospires (6). Briefly, 10 µL of mAb-coated beads were added to clinical and control
21 samples. The immunocapture complex was washed three times, suspended in DNA extraction
22 buffer, boiled and used on PCR assay. To perform the experiments, an immunomagnetic
23 separator MPC-S (Invitrogen, CA, USA) was used.

24 All 5 dog serum samples were MAT positive with titers that varied from 100 to
25 3200. The antibodies most frequently found in the MAT recognized serovars Canicola

1 CCZ463 (5/5), Canicola Hond Utrecht IV (4/5), Icterohaemorrhagiae (4/5), Copenhageni
 2 (4/5), Ballum (3/5) and Grippotyphosa (3/5). The highest agglutination titers corresponded to
 3 serovars Canicola CCZ463 and Canicola Hond Utrecht IV. No agglutination was observed in
 4 sera from healthy dogs. Conventional PCR assay was able to detect 2 pg per 25 μ L of pure
 5 genomic *Leptospira* DNA and 10^3 cells per mL⁻¹ either in artificially contaminated canine
 6 serum or urine samples (data not shown). When IMS was applied on artificially contaminated
 7 samples prior to PCR the detection limit decreased to 10^2 cells mL⁻¹ (Fig. 1A). No
 8 amplification was observed after IMS-PCR performed with saprophytic strains or *E. coli*, or
 9 when non-sensitized beads were used for IMS with pathogenic strains (data not shown). PCR
 10 performed without previous IMS treatment amplified *lipL32* gene sequence from four urine
 11 and one serum samples (data not shown). The IMS-PCR performed with canine leptospirosis
 12 clinical samples was able to amplify *lipL32* sequence gene in all urine and in two out of five
 13 serum samples tested. These results are demonstrated in Fig. 1B. The IMS-PCR approach
 14 enhanced the PCR method since the conventional PCR failed to detect one positive sample.



15
 16 **Figure 1.** Agarose electrophoresis of IMS-PCR from artificially contaminated and clinical
 17 fluid samples in presence of 0.5 pg of IAC. Panel A, detection limit of *L. interrogans* serovar

1 Canicola strain Hond Utrecht IV in artificially contaminated dog urine samples: M, 1 kb DNA
2 Ladder; Lanes 1-7, 10^6 , 10^5 , 10^4 , 10^3 , 10^2 , 10^1 , 10^0 leptospires per mL, respectively; lane 8,
3 DNA only, lane 9, IAC only. Panel B, detection of *Leptospira* spp. amplified from dog
4 clinical samples. M, 1kb DNA Ladder; lane 1-5 (urine) and 6-10 (blood), respectively. Lane
5 11 DNA only; Lane 12 IAC only.

6

7 Canine leptospirosis has a variable clinical presentation but, as a consensus, it results
8 in leptospira renal scarring (5). The recommended diagnostic test has to be done by testing
9 paired acute and convalescent sera to confirm the diagnosis, which is helpful in unvaccinated
10 dogs, but hard to interpret in vaccinated ones (6). The antibodies detection methods are not
11 useful before seven days after leptospira infection and the standard method, MAT; require
12 paired samples to detect seroconversion (5). For those reasons, antigen detection tests offer
13 potential advantage over tests based on antibody detection both for early diagnosis and
14 identification of renal carrier status (5). Therefore, research focused on highly sensitive and
15 specific routine tests for leptospira detection in blood and urine samples led to development of
16 several molecular methods for diagnosis of leptospirosis (4, 6, 9, 14). However, the sensitivity
17 and kinetics of PCR diagnostic tests may be dramatically reduced when applied directly to
18 biological samples, such as urine and serum samples (11). The presence of inhibitor
19 molecules and heterogeneous bacteria in the samples can affect PCR performance (13).

20 Here, we demonstrated that the IMS step can be useful for concentrating leptospires
21 in clinical samples to allow detection by PCR and for reducing inhibitory substances which
22 led to increase in sensitivity. Although the IMS-PCR was able to detect leptospires in only
23 two out of five serum samples tested, high agglutination antibodies titers were found in those
24 sera and no spirochetes were visualized under DFM suggesting absence of leptospiremia in

1 those animals. The use of a sensitive leptospira detection method such as the IMS-PCR, may
2 constitute an important tool for identification of leptospira renal scarring.

3 In conclusion, this study demonstrated that IMS using an extensively characterized
4 mAb against LipL32, a surface exposed outer membrane protein present in all pathogenic
5 leptospires, is efficient in capturing pathogenic leptospiral cells. In addition, the IMS coupled
6 to PCR has the potential to improve sensitivity and specificity of a diagnostic test for
7 leptospirosis. The same approach may be useful for detection of other pathogens.

8

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1 **5. CONCLUSÕES**

2

3 • Os nanocompósitos magnéticos sintetizados a base de carbono e cobalto foram

4 capazes de ancorar diferentes proteínas e auxiliar a captura e detecção de leptospiras

5 patogênicas;

6

7 • A introdução da técnica de IMS utilizando os nanocompósitos magnéticos de

8 poliestireno e ferro, como passo anterior a PCR, aumentou o limite de detecção da

9 PCR a partir de amostras artificialmente contaminadas e a sensibilidade a partir de

10 fluídos biológicos de cães positivos para a leptospirose.

11

12

1 **6. PERSPECTIVAS**

2

3 - Produção de anticorpos policlonais contra *Mycoplasma hyopneumoniae*, *Mycoplasma hyorhinis* e

4 *Mycoplasma flocculare* visando à detecção e isolamento de *M. hyopneumoniae*;

5

6 - Avaliar a técnica de IMS/PCR utilizando os anticorpos produzidos para detectar *M.*
7 *hyopneumoniae* a partir de cultivos puros, artificialmente contaminados com outros micro-
8 organismos e amostras clínicas;

9

10 - Avaliar a técnica de IMS/isolamento utilizando os anticorpos produzidos para isolar *M.*
11 *hyopneumoniae* a partir de cultivos puros, artificialmente contaminados com outros micro-
12 organismos e amostras clínicas;

13

14 - Avaliação dos anticorpos anti-*M. hyorhinis* e anti-*M. flocculare* em ensaios de inibição do
15 crescimento, visando otimizar o isolamento de *M. hyopneumoniae*;

16

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